



## Optimization methods for phase estimation in differential-interference-contrast (DIC) microscopy

Simone Rebegoldi, Lola Bautista, Laure Blanc-Féraud, Marco Prato, Luca Zanni, Arturo Plata

► **To cite this version:**

Simone Rebegoldi, Lola Bautista, Laure Blanc-Féraud, Marco Prato, Luca Zanni, et al.. Optimization methods for phase estimation in differential-interference-contrast (DIC) microscopy. Workshop on Optimization Techniques for Inverse Problems III, Sep 2016, Modena, Italy. hal-01426317

**HAL Id: hal-01426317**

**<https://hal.inria.fr/hal-01426317>**

Submitted on 4 Jan 2017

**HAL** is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers.

L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.

# Optimization methods for phase estimation in differential-interference-contrast (DIC) microscopy

Simone Rebegoldi<sup>1</sup>, Lola Bautista<sup>2,3</sup>, Laure Blanc-Féraud<sup>3</sup>, Marco Prato<sup>1</sup>, Luca Zanni<sup>1</sup> and Arturo Plata<sup>2</sup>

<sup>1</sup>Università di Modena e Reggio Emilia, <sup>2</sup>Universidad Industrial de Santander, <sup>3</sup>Université Côte d'Azur,

## The DIC phase estimation problem

Differential Interference Contrast Schematic

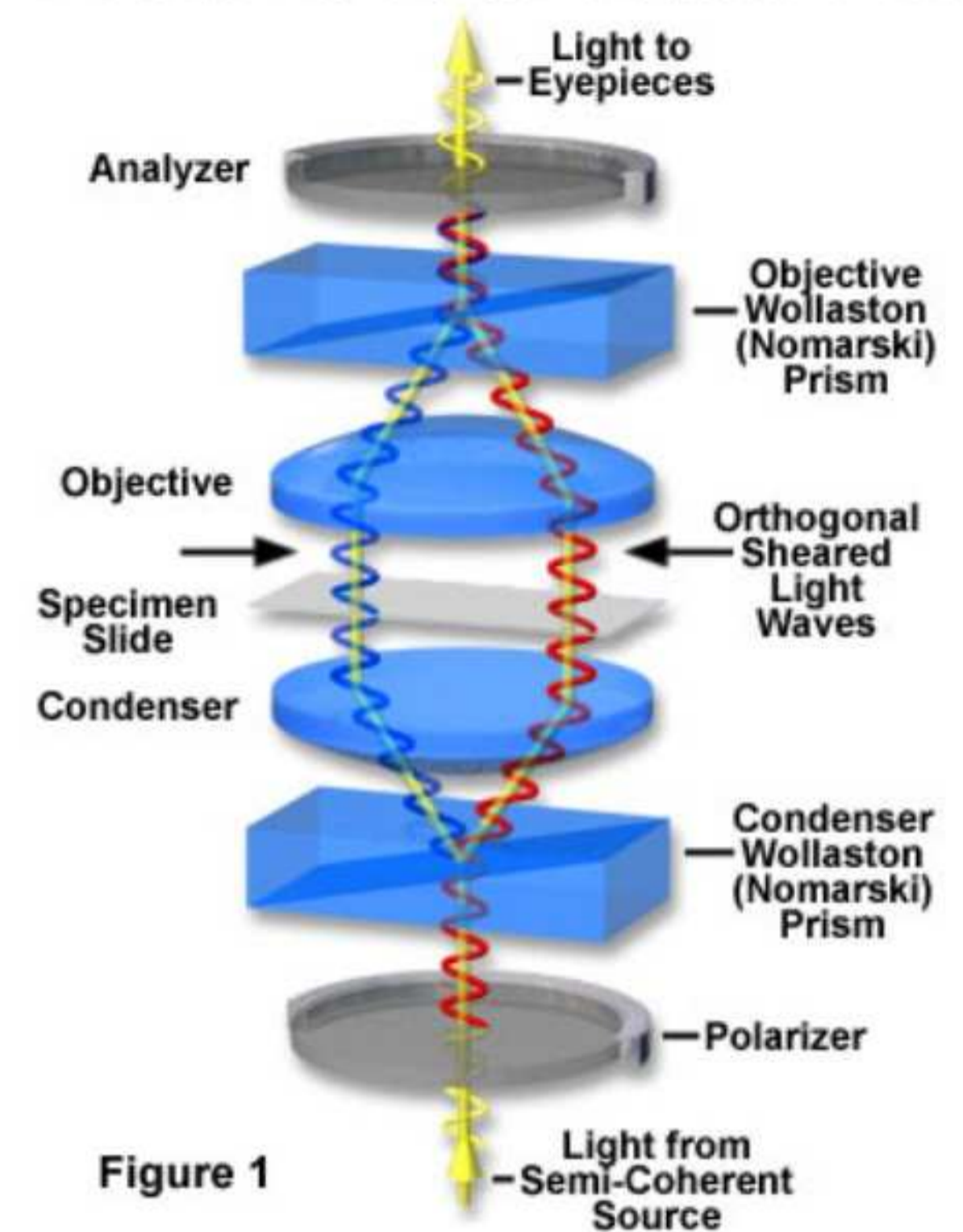
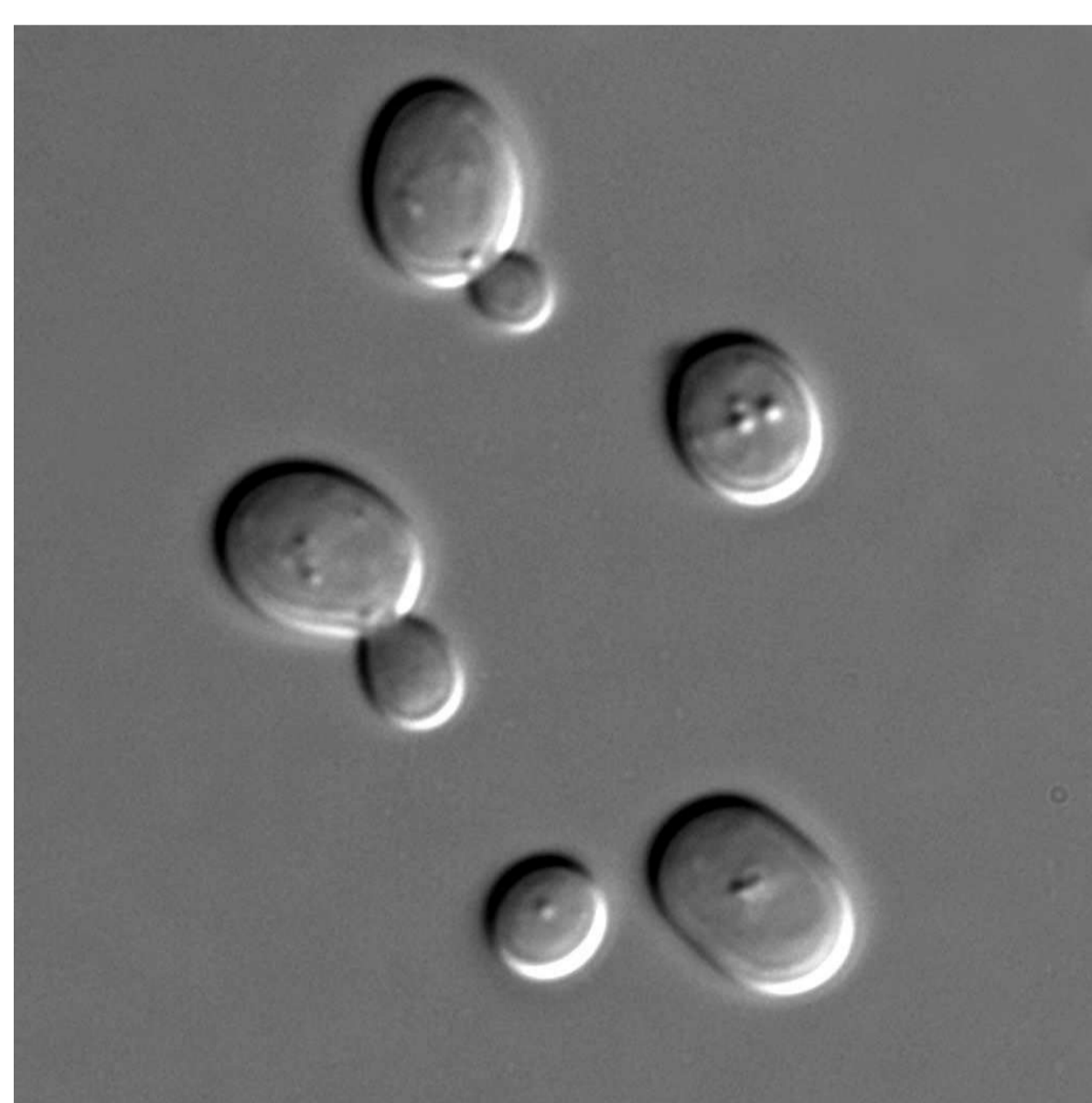


Figure 1



The DIC image is formed by the interference of two orthogonally polarized beams that have a lateral displacement (called *shear*) and are phase shifted relatively one to each other. The resulting image has a 3D high contrast appearance, which can be enhanced by introducing a uniform phase difference between the beams (called *bias*).

**Model:** the DIC image formation is described by the polychromatic rotational-diversity model [1,2]

$$(o_{k,\lambda_\ell})_j = \left| (h_{k,\lambda_\ell} \otimes e^{-i\phi/\lambda_\ell})_j \right|^2 + (\eta_{k,\lambda_\ell})_j, \quad k = 1, \dots, K, \ell = 1, 2, 3, j \in \chi$$

- $k$  is the index of the rotation of the specimen w.r.t. the horizontal axis,  $\ell$  is the index denoting one of the RGB channels and  $j = (j_1, j_2)$  is a 2D-index varying in the set  $\chi = \{1, \dots, M\} \times \{1, \dots, P\}$
- $\lambda_\ell$  is the  $\ell$ -th illumination wavelength
- $o_{k,\lambda_\ell} \in \mathbb{R}^{MP}$  is the  $\ell$ -th color component of the  $k$ -th observed image  $o_k = (o_{k,\lambda_1}, o_{k,\lambda_2}, o_{k,\lambda_3}) \in \mathbb{R}^{MP \times 3}$
- $\phi \in \mathbb{R}^{MP}$  is the unknown phase vector and  $e^{-i\phi/\lambda_\ell} \in \mathbb{C}^{MP}$  is defined by  $(e^{-i\phi/\lambda_\ell})_j = e^{-i\phi_j/\lambda_\ell}$
- $h_{k,\lambda_\ell} \in \mathbb{C}^{MP}$  is the discretization of the continuous DIC Point Spread Function
- $\eta_{k,\lambda_\ell} \in \mathbb{R}^{MP}$  is the noise corrupting the data,  $\eta_{k,\lambda_\ell} \sim \mathcal{N}(\mathbf{0}, \sigma^2 I_{(MP)^2})$ .

**Problem:** given the rotationally diverse images  $o_1, \dots, o_K$ , retrieve the phase vector  $\phi$  by solving

$$\min_{\phi \in \mathbb{R}^{MP}} J(\phi) \equiv J_0(\phi) + J_{TV}(\phi), \quad (\text{P})$$

- $J_0(\phi) = \sum_{\ell=1}^3 \sum_{k=1}^K \sum_{j \in \chi} \left[ (o_{k,\lambda_\ell})_j - \left| (h_{k,\lambda_\ell} \otimes e^{-i\phi/\lambda_\ell})_j \right|^2 \right]^2$  is the nonconvex least-squares term
- $J_{TV}(\phi) = \mu \sum_{j \in \chi} \sqrt{((\mathcal{D}\phi)_{j_1})^2 + ((\mathcal{D}\phi)_{j_2})^2 + \delta^2}$  is the total variation (TV) functional, where  $\mu > 0$  is the regularization parameter and  $\delta \geq 0$  is the smoothing parameter ( $\delta = 0 \rightarrow$  standard TV).

## Optimization methods

**Case  $\delta > 0$ :** problem (P) is differentiable  $\rightarrow$  we use a gradient-descent method.

**Algorithm 1** Limited Memory Steepest Descent (LMSD) method [3]

Set  $\rho, \omega \in (0, 1)$ ,  $m > 0$ ,  $\alpha_0^{(0)}, \dots, \alpha_{m-1}^{(0)} > 0$ ,  $\phi^{(0)} \in \mathbb{R}^{MP}$ ,  $G = [\ ]$ ,  $\Theta = [\ ]$ ,  $n = 0$ .

WHILE True

FOR  $l = 1, \dots, m$

1. Compute the smallest non-negative integer  $i_n$  such that  $\alpha_n = \alpha_n^{(0)} \rho^{i_n}$  satisfies

$$J(\phi^{(n)} - \alpha_n \nabla J(\phi^{(n)})) \leq J(\phi^{(n)}) - \omega \alpha_n \|\nabla J(\phi^{(n)})\|^2.$$

2. Compute the new point as  $\phi^{(n+1)} = \phi^{(n)} - \alpha_n \nabla J(\phi^{(n)})$ .

3. Update  $G = [G \ \nabla J(\phi^{(n)})]$  and  $\Theta = [\Theta \ \alpha_n^{-1}]$ .

4. Set  $n = n + 1$ .

END

6. Define the  $(m+1) \times m$  matrix  $\Gamma = \begin{bmatrix} \text{diag}(\Theta) \\ \text{zeros}(1, m) \end{bmatrix} - \begin{bmatrix} \text{zeros}(1, m) \\ \text{diag}(\Theta) \end{bmatrix}$ .

7. Compute the Cholesky factorization  $R^T R$  of the  $m \times m$  matrix  $G^T G$ .

8. Solve the linear system  $R^T r = G^T \nabla J(\phi^{(n)})$ .

9. Define the  $m \times m$  matrix  $\Phi = [R, r] \Gamma R^{-1}$  and its approximation

$$\tilde{\Phi} = \text{diag}(\Phi) + \text{tril}(\Phi, -1) + \text{tril}(\Phi, -1)^T,$$

which is symmetric and tridiagonal.

10. Compute eigenvalues  $\theta_1, \dots, \theta_m$  of  $\tilde{\Phi}$  and define  $\alpha_{n+i-1}^{(0)} = 1/\theta_i$ ,  $i = 1, \dots, m$ .

END

**Case  $\delta = 0$ :** problem (P) is non differentiable  $\rightarrow$  we use a proximal-gradient method.

**Algorithm 2** Inexact Linesearch based Algorithm (ILA) [4]

Set  $\rho, \omega \in (0, 1)$ ,  $0 < \alpha_{\min} \leq \alpha_{\max}$ ,  $\tau > 0$ ,  $\phi^{(0)} \in \mathbb{R}^{MP}$ ,  $n = 0$ .

WHILE True

1. Set  $\alpha_n = \max \left\{ \min \left\{ \alpha_n^{(0)}, \alpha_{\max} \right\}, \alpha_{\min} \right\}$ , where  $\alpha_n^{(0)}$  is chosen as in Algorithm 1.

2. Let  $\psi^{(n)} = \text{prox}_{\alpha_n J_{TV}}(\phi^{(n)} - \alpha_n \nabla J_0(\phi^{(n)})) = \text{argmin}_{\phi \in \mathbb{R}^{MP}} h^{(n)}(\phi)$ .

Compute  $\tilde{\psi}^{(n)}$  such that  $h^{(n)}(\tilde{\psi}^{(n)}) - h^{(n)}(\psi^{(n)}) \leq \epsilon_n$  and  $0 \leq \epsilon_n \leq -\tau h^{(n)}(\tilde{\psi}^{(n)})$ .

3. Set  $d^{(n)} = \tilde{\psi}^{(n)} - \phi^{(n)}$ .

4. Compute the smallest non-negative integer  $i_n$  such that  $\lambda_n = \rho^{i_n}$  satisfies

$$J(\phi^{(n)} + \lambda_n d^{(n)}) \leq J(\phi^{(n)}) + \omega \lambda_n h^{(n)}(\tilde{\psi}^{(n)}).$$

5. Compute the new point as  $\phi^{(n+1)} = \phi^{(n)} + \lambda_n d^{(n)}$ .

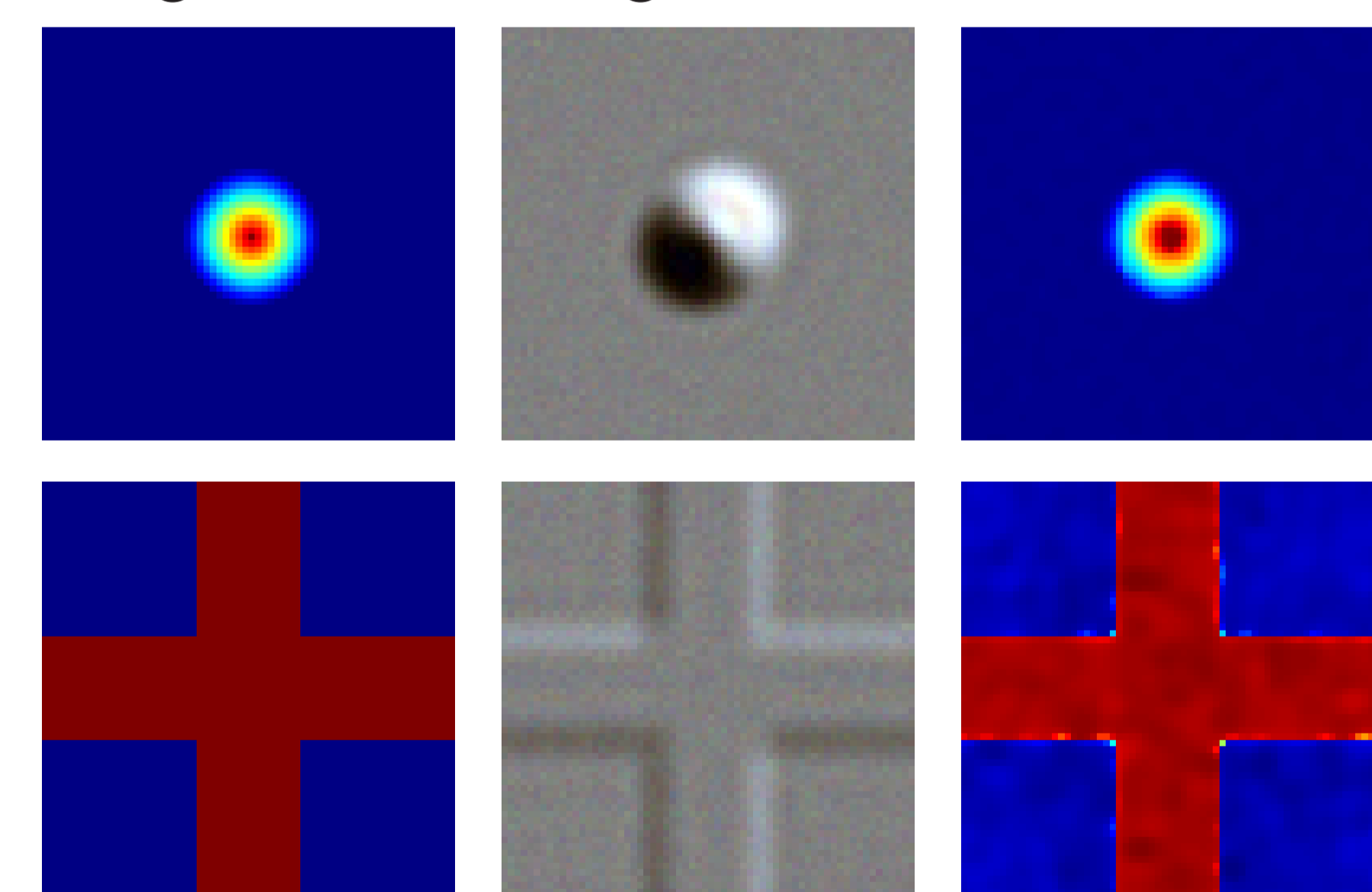
6. Set  $n = n + 1$ .

END

## Convergence and numerical results

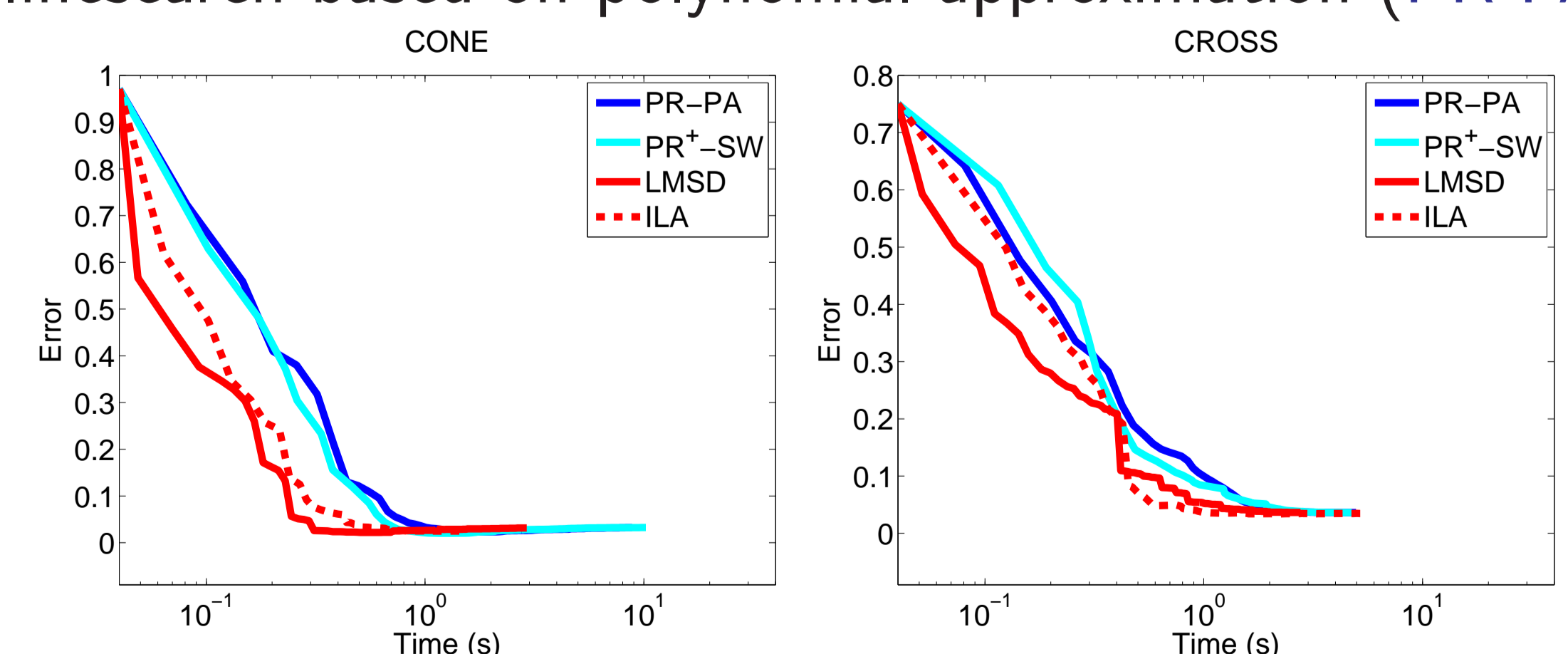
**Convergence:** Any limit point of Algorithm 1 and 2 is stationary for problem (P). Since  $J$  satisfies the Kurdyka-Łojasiewicz property, Algorithm 1 converges to a limit point; the same result can be proved for Algorithm 2 when the proximal point is computed exactly [4].

**Results:** for both objects, cone (top row) and cross (bottom row),  $K = 2$  DIC images have been generated.



True phase Noisy DIC image Rec. phase

The parameters of the methods have been tuned as follows:  $\rho = 0.5$ ,  $\omega = 10^{-4}$ ,  $m = 4$ ,  $\alpha_{\min} = 10^{-5}$ ,  $\alpha_{\max} = 10^2$ ,  $\tau = 10^6 - 1$ ,  $\phi^{(0)} = 0$ . The methods are compared with the Polak-Ribière conjugate gradient method equipped with the strong Wolfe conditions (PR<sup>+</sup>-SW) and a linesearch based on polynomial approximation (PR-PA) [1].



Object	Algorithm	Iterations	# f	# g	Error
Cone	PR-PA	98	997	98	3.63 %
	PR <sup>+</sup> -SW	98	326	326	3.63 %
	LMSD	152	221	152	3.64 %
	ILA	97	179	97	3.46 %

[1] C. Preza, J. Opt. Soc. Am. A, 17(3), 415–424, 2000.

[2] L. Bautista et al., 2016 IEEE 13th Int. Symp. on Biomedical Imaging, 136–139, 2016.

[3] R. Fletcher, Math. Program., 135(1–2), 413–436, 2012.

[4] S. Bonettini et al., ArXiv: 1605.03791, 2016.